



Deformable Image Registration with Implicit Neural Representations

Seminar: Deep Learning for Medical Applications

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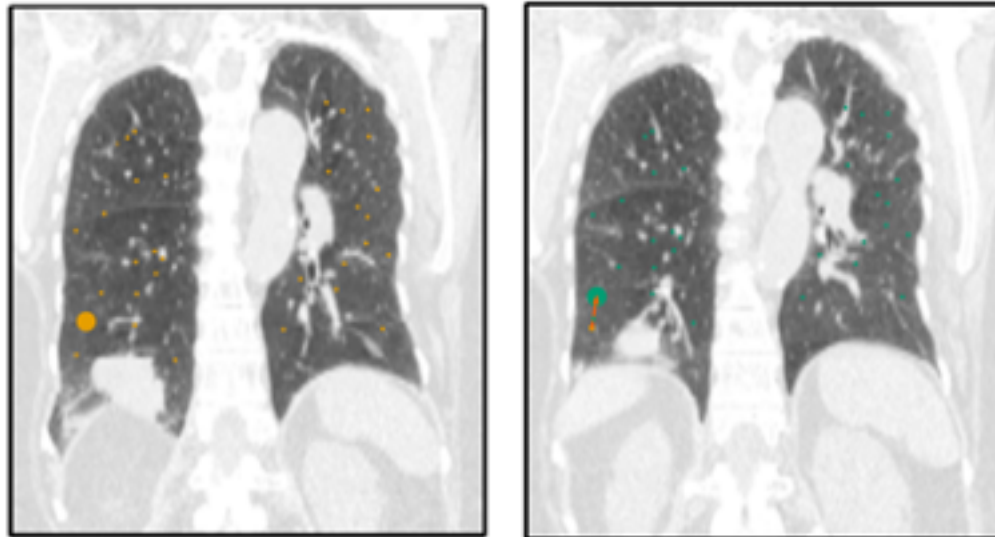
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Introduction



Problem of Interest



Images adapted from [1]

Can we find the matching point between images?



Deformable Image Registration

- Aligning corresponding semantic regions across images
- Non-rigid deformations

- **Applications**
 - Motion analysis
 - Multi-modal image analysis
 - Disease tracking



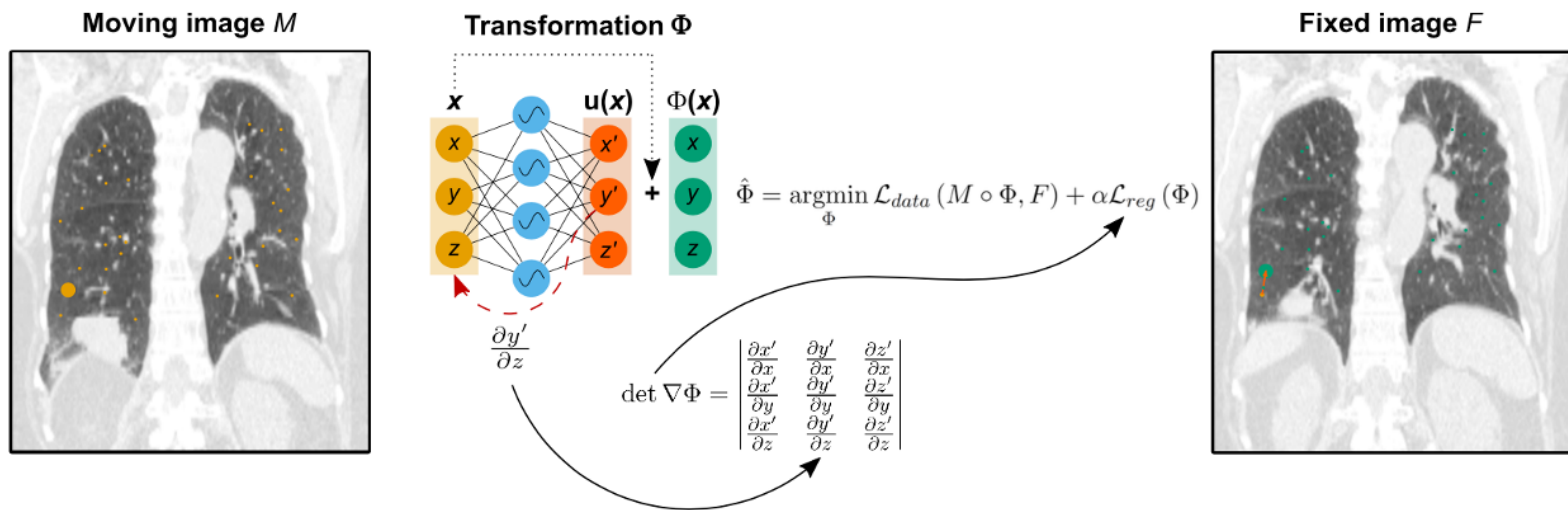
Deformable Image Registration

- **Conventional Iterative Methods:** mathematical modals
 - Effective
 - High computational resources
 - Sensitive to noise
- **Data-driven Methods:** deep learning architectures
 - Fast inference
 - Reduced accuracy
 - Large training data
 - Resolution dependency
 - Generalization failure



Implicit Neural Representations (INRs)

- Implicitly represent continuous signals as a function stored in the weights of a multi-layer perceptron [2]



Schematic Overview of INRs for Image Registration [1]



[1] J. M. Wolterink, J. C. Zwienenberg, and C. Brune. "Implicit neural representations for deformable image registration". In: International Conference on Medical Imaging with Deep Learning . PMLR, 2022, pp. 1349–1359.
 [2] V. Sitzmann, J. Martel, A. Bergman, D. Lindell, and G. Wetzstein. "Implicit neural representations with periodic activation functions". In: Advances in neural information processing systems 33 (2020), pp. 7462–7473.

Implicit Neural Representations (INRs)

- **Advantages**

- Continuous representation
- Memory efficiency
- Accurate gradients
- Pair-wise optimization

- **Challenges**

- Complex deformations
- Spatial folding
- Failure due to non-convex optimization



Motivation





Paper Summaries



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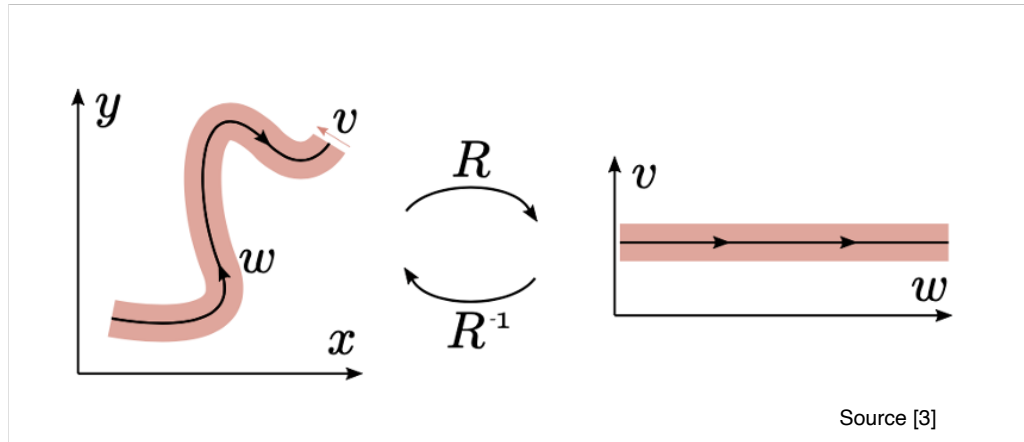


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Geometry-Informed INRs [3]

Research Problem

Complex deformations → Simplify deformation function via geometric alignment



Geometry-Informed INRs

Method

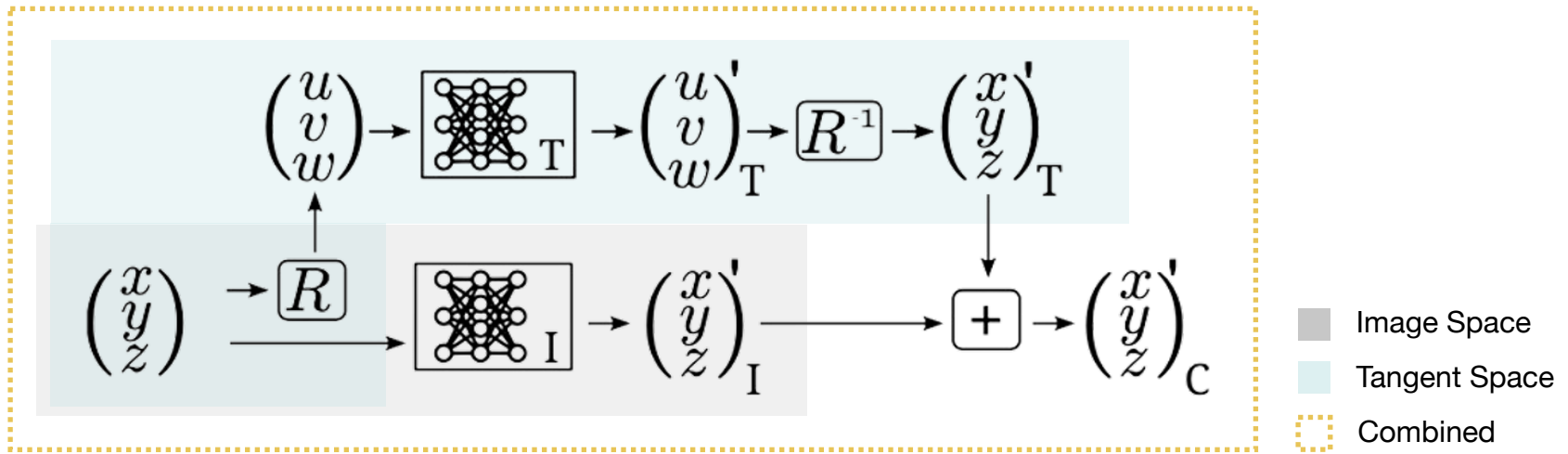
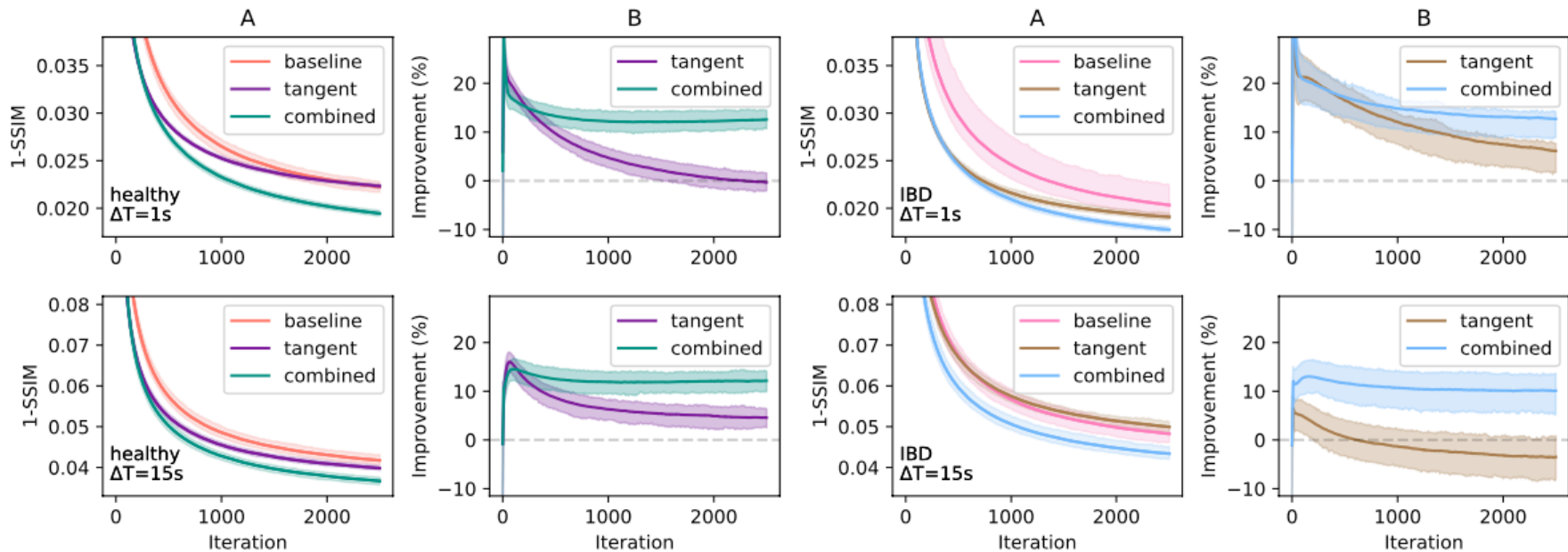


Image adapted from [3]



Geometry-Informed INRs

Experiments & Results: Quantitative



Source [3]



Geometry-Informed INRs

Experiments & Results: Qualitative

Bowel motility as dominant motion → beneficial

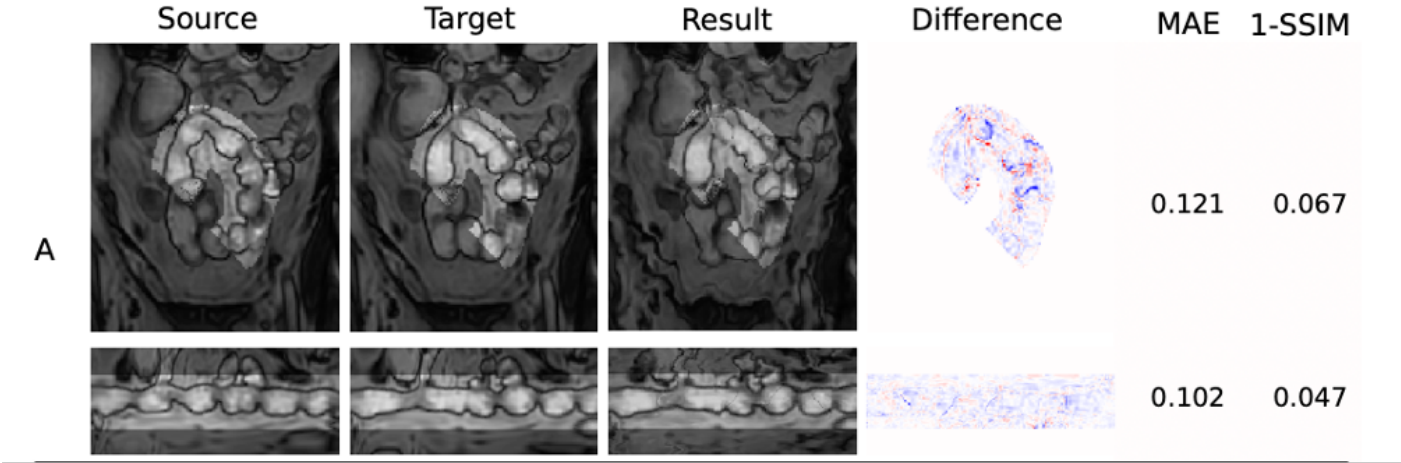


Image adapted from [3]



[3] L. van Harten, R. L. M. Van Harten, J. Stoker, and I. Isgum. "Deformable Image Registration with Geometry-informed Implicit Neural Representations". In: Medical Imaging with Deep Learning . PMLR. 2024, pp. 730–742.

Geometry-Informed INRs

Experiments & Results: Qualitative

- Centerline inaccurately extracted
 - Motility absent
- ➔ not beneficial

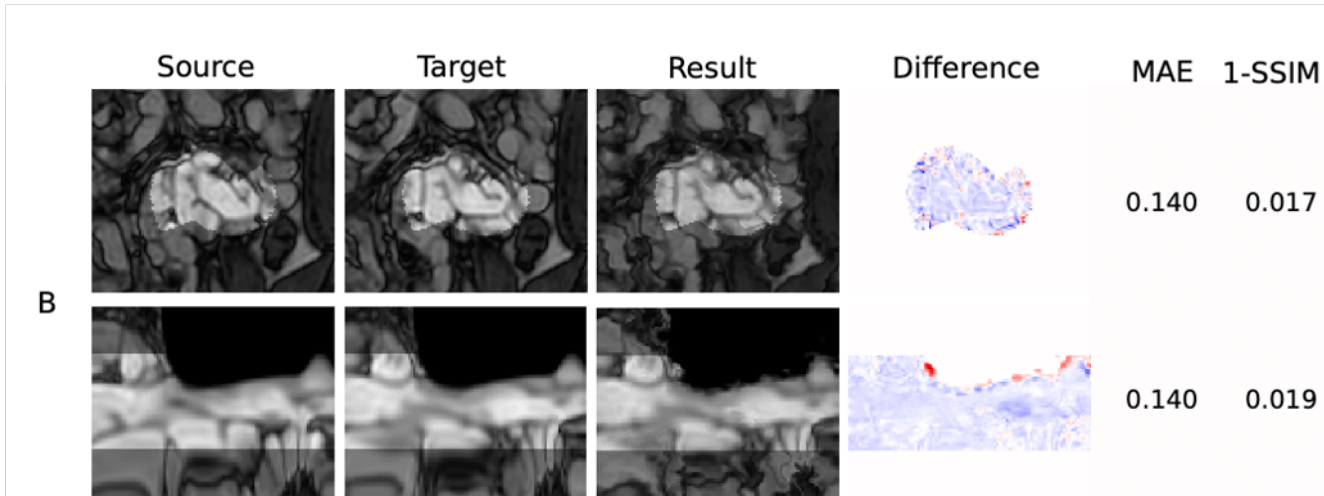


Image adapted from [3]



Geometry-Informed INRs

Experiments & Results: Qualitative

Breathing becomes the dominant motion → harmful

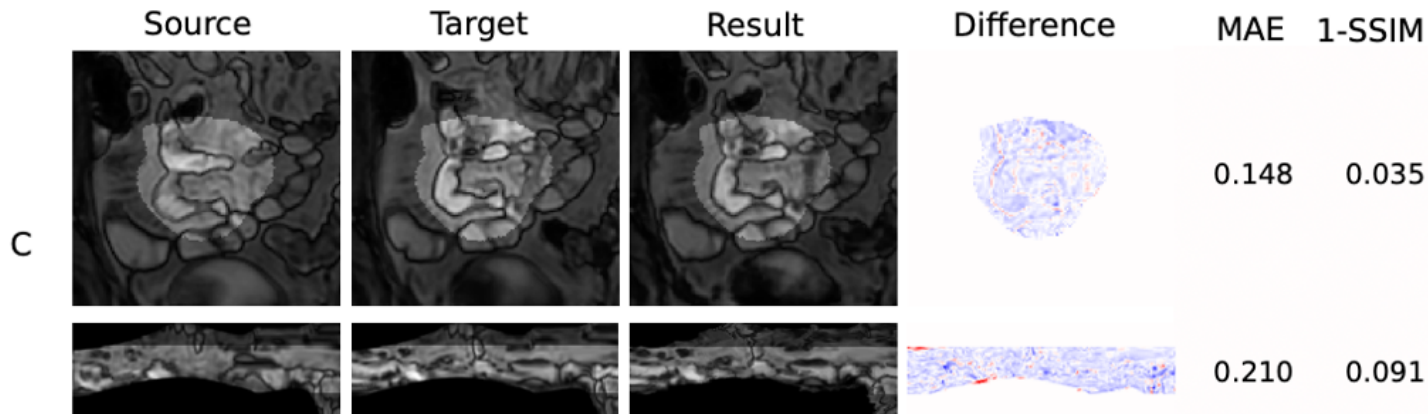


Image adapted from [3]



Geometry-Informed INRs [3]

Discussion

- **Advantages**

- improved registration accuracy for bowel loops with active motility;
- accuracy further improved with the combined model;
- improved efficiency;
- potential application in other areas, e.g. cardiac motion, ischemic stroke follow-up

- **Limitations**

- additional resources for centerline extraction;
- limited / negative impact due to bad centerline extraction or dominant breathing motion;
- generalisability questionable without further test;



SINR: Spline-enhanced INR [4]

Research Problem

- Spatial folding
- Sampling method not optimal for multi-modal registration



Combining B-spline Free Form Deformation (FFD) [5] with INRs for smooth transformations



SINR: Spline-enhanced INR

Method: FFD

- Control points
- B-spline basis functions
- Smooth deformations

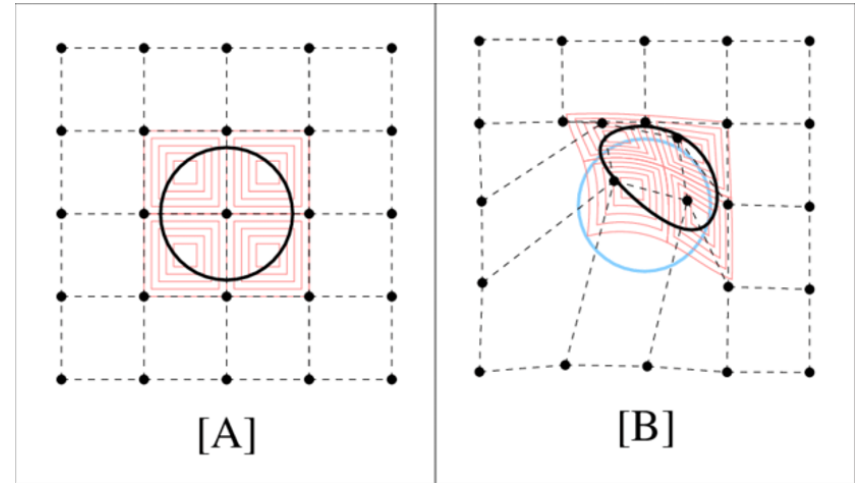
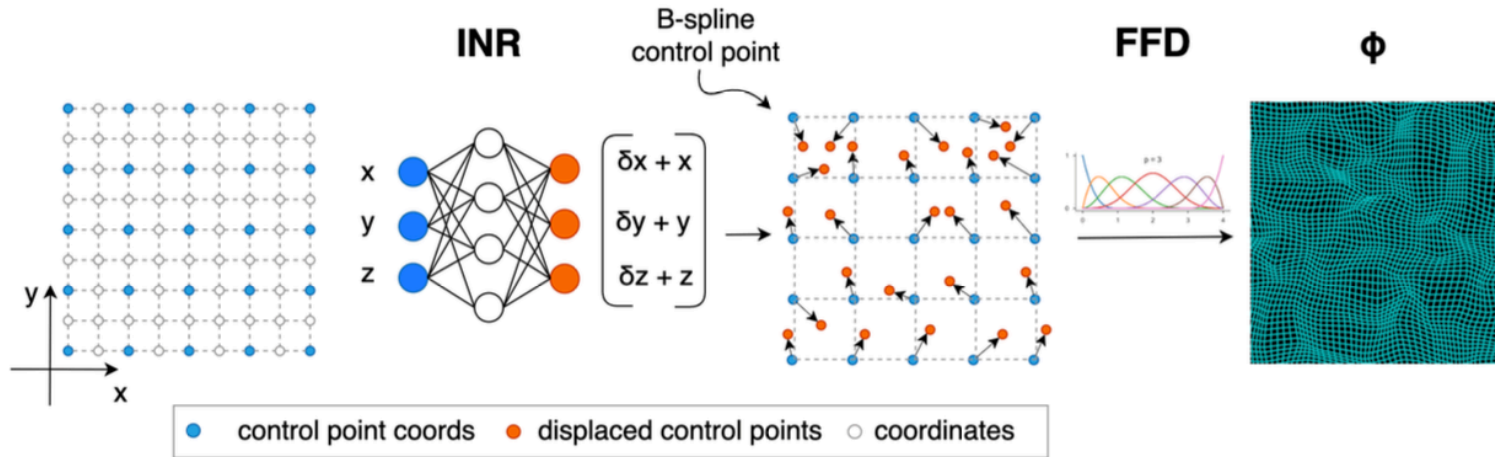


Image adapted from [6]



SINR: Spline-enhanced INR

Method: Schematic Overview



Source [4]



SINR: Spline-enhanced INR

Experiments & Results: Quantitative Overview

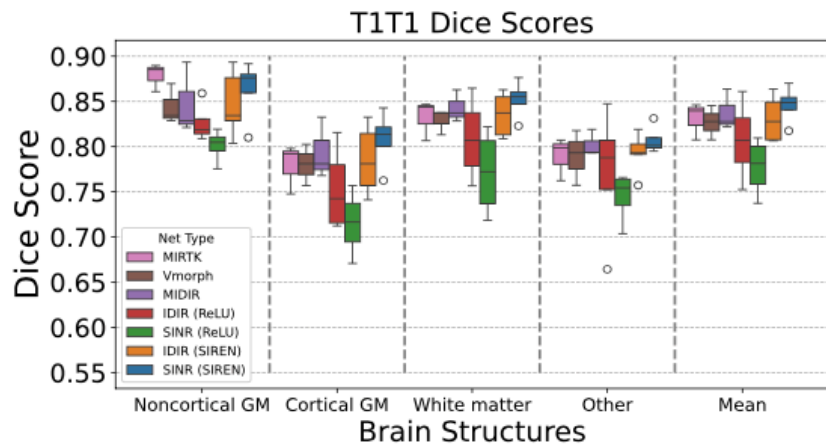
Method	T1w-T1w CamCAN			T1w-T2w CamCAN	
	FFD	Dice \pm std \uparrow	Folding % \downarrow	Dice \pm std \uparrow	Folding % \downarrow
Affine	n/a	0.619 \pm 0.01	-	0.619 \pm 0.01	-
MIRTK	✓	0.833 \pm 0.02	0.11	0.755 \pm 0.01	0.14
VMorph [CNN]	✗	0.812 \pm 0.06	0.31	0.733 \pm 0.04	0.19
MIDIR [CNN]	✓	0.817 \pm 0.06	0.23	0.735 \pm 0.04	0.12
IDIR [ReLU-MLP]	✗	0.806 \pm 0.02	0.44	0.683 \pm 0.03	0.15
SINR [ReLU-MLP]	✓	0.789 \pm 0.03	0.38	0.721 \pm 0.06	0.05
IDIR [SIREN]	✗	0.837 \pm 0.05	0.84	0.736 \pm 0.02	0.81
SINR [SIREN]	✓	0.855 \pm 0.06	0.59	0.784 \pm 0.04	0.27

Source [4]

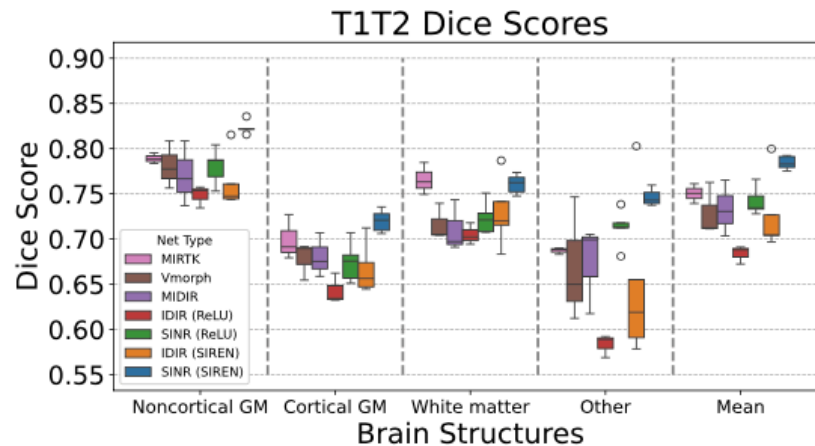


SINR: Spline-enhanced INR

Experiments & Results: Quantitative by Structure



(a) T1w-T1w



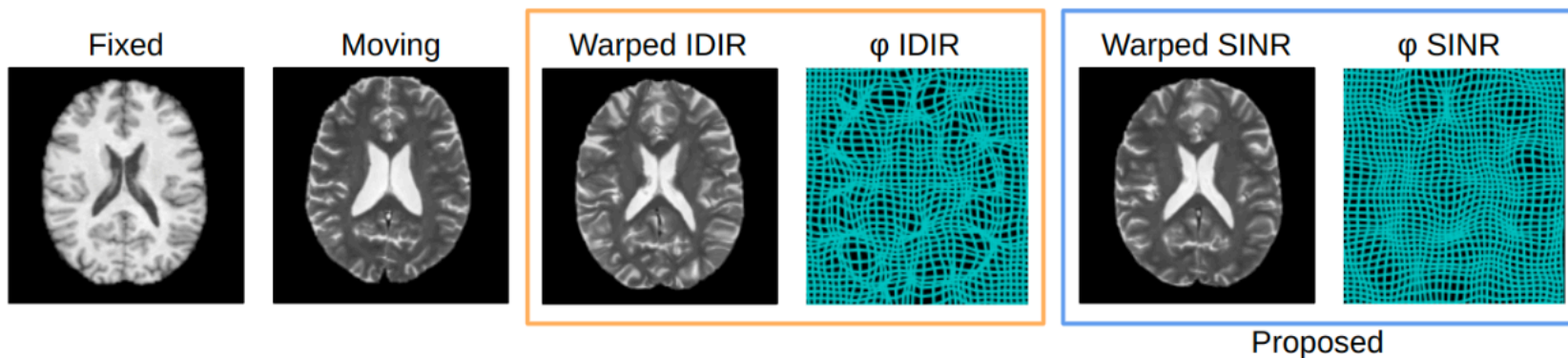
(b) T1w-T2w

Source [4]



SINR: Spline-enhanced INR

Experiments & Results: Qualitative



Source [4]



SINR: Spline-enhanced INR

Discussion

- **Advantages**

- higher Dice score than existing methods;
- reduced folding ratio for INR-based method;
- efficient spatial sampling and calculation of metrics for multi-modal registration.

- **Limitations**

- higher folding ratio compared to conventional and CNN-based methods;
- balance between the accuracy and folding ratio yet to be explored;
- generalisability questionable without further test.



Cycle-Consistent INRs [7]

Research Problem

- Failure due to non-convex optimization
- Sensitive to initialization settings

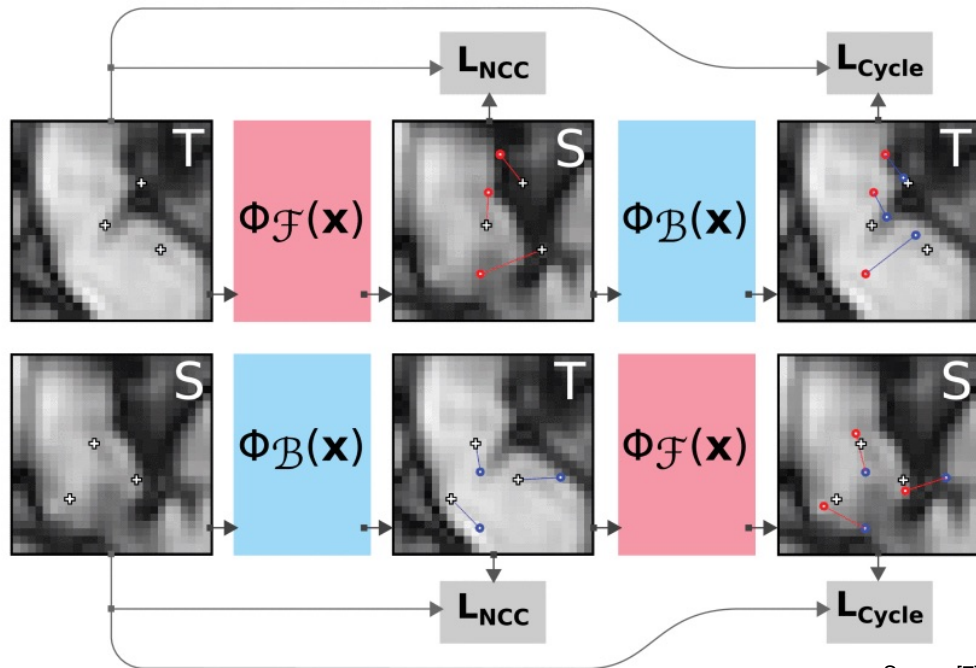


Using forward-backward cycle-consistency to improve robustness



Cycle-Consistent INRs

Method: Optimization

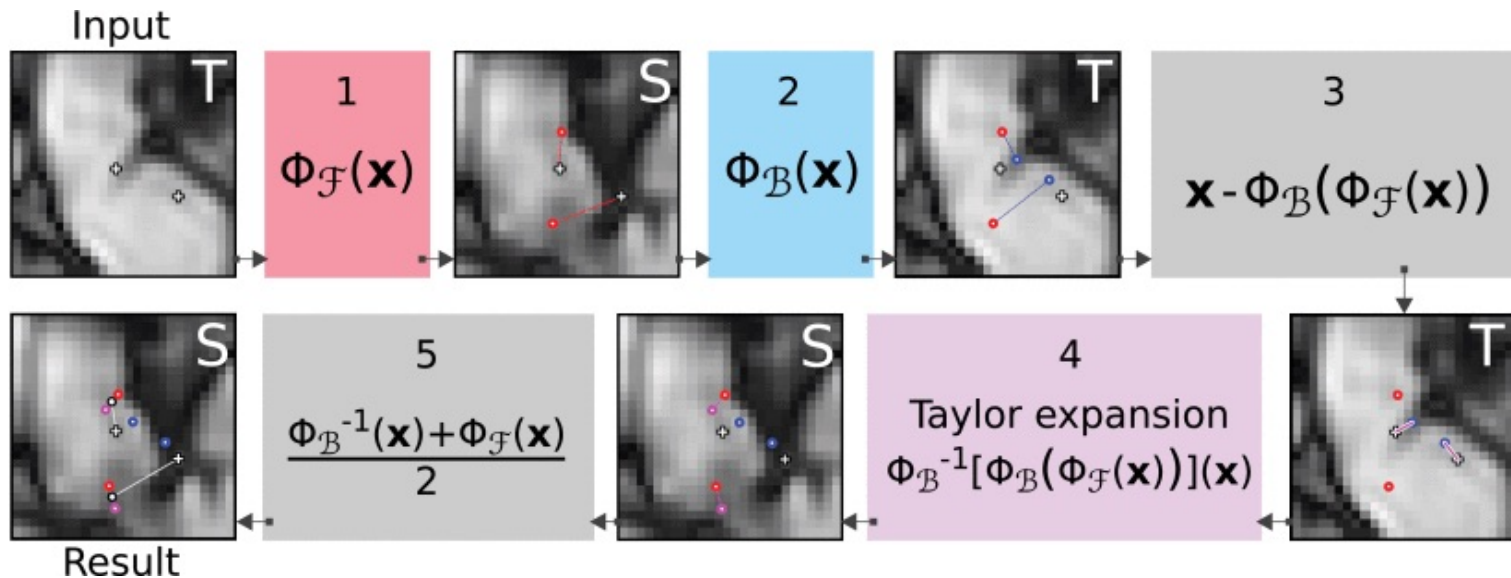


Source [7]



Cycle-Consistent INRs

Method: Inference



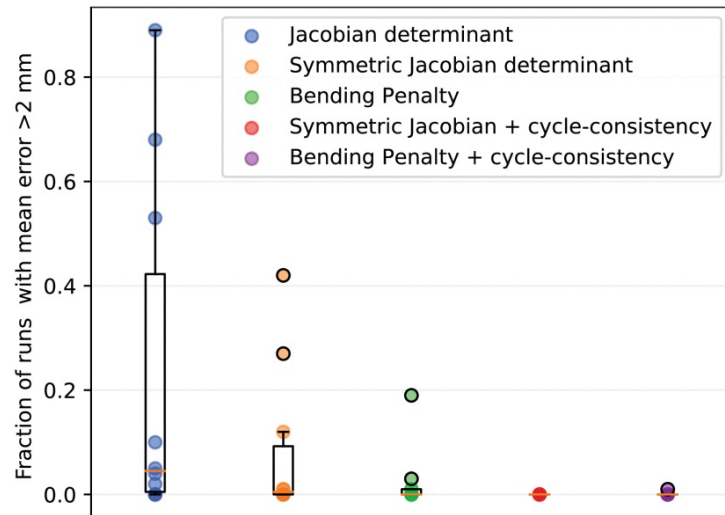
Source [7]



Cycle-Consistent INRs

Experiments & Results: Lung CT Data

Method	mean \pm std (mm)
DLIR [7]	2.64 ± 4.32
VoxelMorph [8]	2.26 ± 2.30
CycleMorph [21]	2.19 ± 2.26
CNN with anatomical constraints [29]	1.14 ± 0.76
Uniform B-Splines [30]	1.36 ± 1.01
CorrField [31]	1.12 ± 1.08
Keypoint correspondence optimization [32]	0.94 ± 1.06
● INR + Symmetric Jacobian det.	1.27 ± 2.27
● INR + Bending penalty	1.10 ± 1.42
● INR + Symmetric Jacobian det. + cycle	1.04 ± 1.11
● INR + Bending penalty + cycle	1.06 ± 1.34



Source [7]



Cycle-Consistent INRs

Experiments & Results: Sensitivity to Hyperparameters

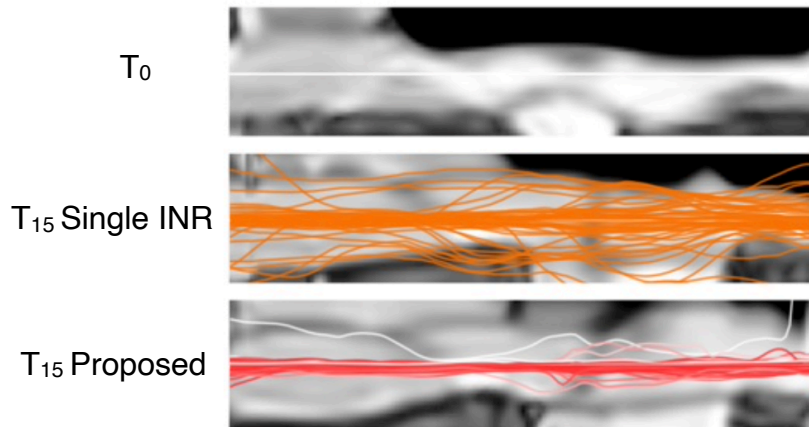
Setting	TRE (mm)	Failure rate (%)
Single INR ($\alpha = 0.05, \beta = 0$)	1.14	8.3
Proposed ($\alpha = 0.05, \beta = 1e-3$)	1.07	0
Jacobian det. $\alpha = 0.50$	1.11	0
Jacobian det. $\alpha = 0.10$	1.08	0
Jacobian det. $\alpha = 0.025$	1.07	0.3
Jacobian det. $\alpha = 0.005$	1.07	1.8
cycle $\beta = 1e-2$	1.08	0.4
cycle $\beta = 2e-3$	1.07	0
cycle $\beta = 5e-4$	1.07	0
cycle $\beta = 1e-4$	1.06	0.4
ReLU network	1.22	0
No masks	1.11	0

Source [7]



Cycle-Consistent INRs

Experiments & Results: Abdominal MRI Data



Strategy	Discrepancy (mm) \pm stdev			
	1s	5s	10s	15s
Single INR	0.68 ± 0.68	2.26 ± 2.05	2.47 ± 2.05	2.99 ± 2.31
Proposed	0.45 ± 0.54	1.21 ± 1.06	1.48 ± 1.54	1.62 ± 1.57

Source [7]



Cycle-Consistent INRs

Discussion

- **Advantages**

- significantly improved registration accuracy and robustness;
- insensitive to hyperparameter settings;
- introduces an uncertainty metric useful for automatic quality control;
- generalisability tested on two different datasets;
- discussed possible changes for multi-modal registration.

- **Limitations**

- higher computational complexity and runtime;
- limited application with high dimensional data and in real-time applications.





Conclusion



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Conclusion

Summary

Challenge	Approach	Accuracy	Efficiency	Generalisibility
Complex deformations	Geometric prior	+	+	Untested
Spatial folding	Spline-based FFD	+	-	Untested
Optimization failure	Cycle-consistency	+	-	Tested



Conclusion

Future Works

If generalization of INRs can further improve the registration performance?

- General or statistical representation of a structure
- Statistical atlas as regularizer
- Complementary data sources





Thank You for Your Attention

Q & A



Bibliography

- [1] J. M. Wolterink, J. C. Zwanenbergh, and C. Brune. “Implicit neural representations for deformable image registration”. In: International Conference on Medical Imaging with Deep Learning . PMLR. 2022, pp. 1349– 1359.
- [2] V. Sitzmann, J. Martel, A. Bergman, D. Lindell, and G. Wetzstein. “Implicit neural representations with periodic activation functions”. In: Advances in neural information processing systems 33 (2020), pp. 7462–7473.
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- [4] V. Sideri-Lampretsa, J. McGinnis, H. Qiu, M. Paschali, W. Simson, and D. Rueckert. “SINR: Spline-enhanced implicit neural representation for multi-modal registration”. In: Medical Imaging with Deep Learning . 2024.
- [5] D. Rueckert, L. I. Sonoda, C. Hayes, D. L. Hill, M. O. Leach, and D. J. Hawkes. “Nonrigid registration using free-form deformations: application to breast MR images”. In: IEEE transactions on medical imaging 18.8 (1999), pp. 712–721.
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- [7] L. D. Van Harten, J. Stoker, and I. Isgum. “Robust deformable image registration using cycle-consistent implicit representations”. In: IEEE Transactions on Medical Imaging (2023).
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- [9] G. Balakrishnan, A. Zhao, M. R. Sabuncu, J. Guttag, and A. V. Dalca. “Voxelmorph: a learning framework for deformable medical image registration”. In: IEEE transactions on medical imaging 38.8 (2019), pp. 1788– 1800.





Supplemental Slides



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Geometry-Informed INRs

Method: Loss Function

$$\begin{aligned} L &= L^{data} + \alpha L^{jac} \\ &= \frac{1}{bs} \sum_{i=1}^{bs} (-NCC(T[R^{-1}(\bar{x}_i)], S[R^{-1}(\Phi(\bar{x}_i))])) + \alpha |1 - \det \nabla \Phi[\bar{x}_i]|, \end{aligned}$$



SINR: Spline-enhanced INR

Method: FFD

$$\mathbf{u}(x, y, z) = \sum_{l=0}^3 \sum_{m=0}^3 \sum_{n=0}^3 B_l(u) B_m(v) B_n(w) c_{i+l} c_{j+m} c_{k+n},$$

B-spline Basis Functions [5]:

$$B_0(u) = \frac{(1-u)^3}{6}, \quad B_1(u) = \frac{3u^3 - 6u^2 + 4}{6},$$
$$B_2(u) = \frac{-3u^3 + 3u^2 + 3u + 1}{6}, \quad B_3(u) = \frac{u^3}{6}$$

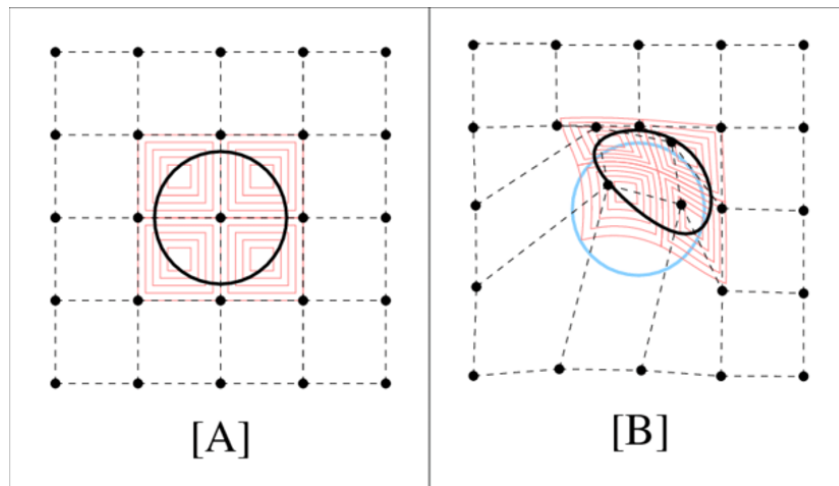
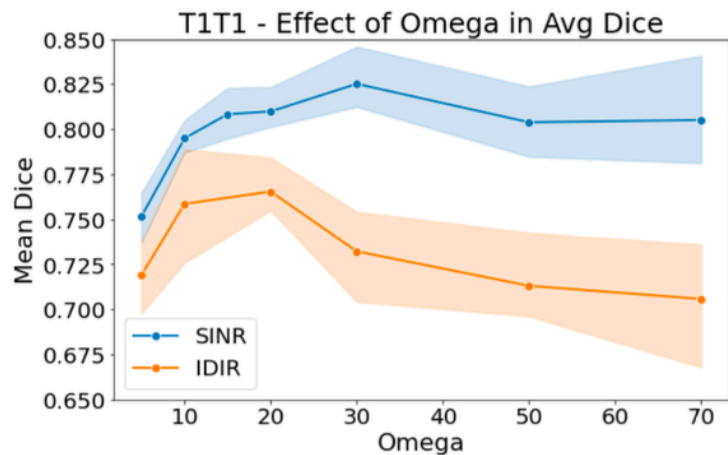


Image adapted from [6]

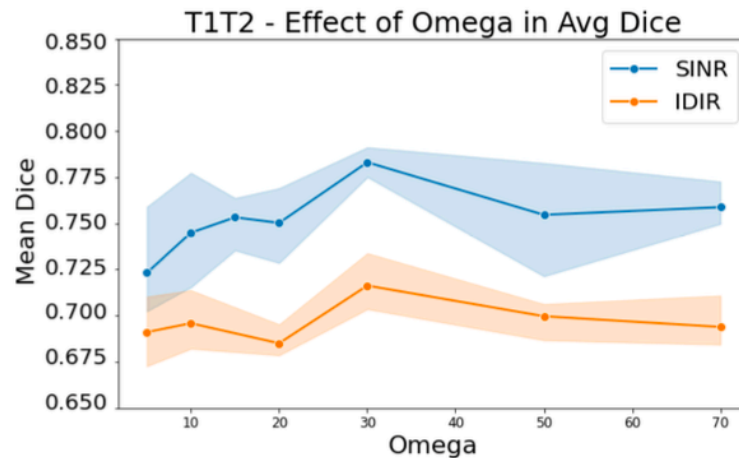


SINR: Spline-enhanced INR

Experiments & Results: Sensitivity to Hyperparameter



(a) T1w-T1w



(b) T1w-T2w

Source [4]



SINR: Spline-enhanced INR

Experiments & Results: Run Time

Table 2: Runtime for mono- and multi-modal registration for all methods.

Method	Runtime↓	
	T1w-T1w CamCAN	T1w-T2w CamCAN
MIRTK	3min 28s	3min 41s
VMorph [CNN]	Train: 15h 23min Test: 219ms	Train: 15h 34min Test: 219ms
MIDIR [CNN]	Train: 12h 55min Test: 113ms	Train: 12h 49min Test: 113ms
IDIR [ReLU-MLP]	Fit: 1min 43s Test: 2.9s	Fit: 2min 01s Test: 2.9s
SINR [ReLU-MLP]	Fit: 1min 54s Test: 2.9s	Fit: 2min 17s Test: 2.9s
IDIR [SIREN]	Fit: 45s Test: 2.9s	Fit: 1min 39s Test: 2.9s
SINR [SIREN]	Fit: 1min 32s Test: 2.9s	Fit: 2min 12s Test: 2.9s

Source [4]



Cycle-Consistent INRs

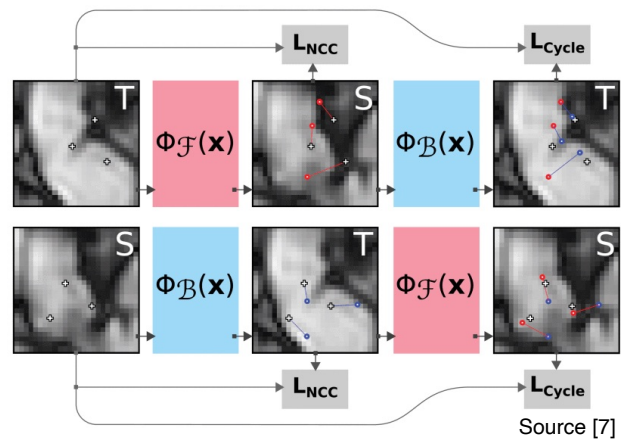
Method: Optimization

$$L_{\text{total}} = L_{\mathcal{F}}^{\text{data}} + \alpha L_{\phi_{\mathcal{F}}}^{\text{reg}} + \beta L_{\mathcal{F} \rightarrow \mathcal{B}}^{\text{cycle}} + L_{\mathcal{B}}^{\text{data}} + \alpha L_{\phi_{\mathcal{B}}}^{\text{reg}} + \beta L_{\mathcal{B} \rightarrow \mathcal{F}}^{\text{cycle}},$$

$$L_{\mathcal{F}}^{\text{data}} = \frac{2}{bs} \sum_{i=1}^{bs/2} -\text{NCC}(S[\vec{x}_i], T[\Phi_{\mathcal{F}}(\vec{x}_i)]),$$

$$L^{\text{sjac}}[\Phi] = \frac{1}{bs} \sum_{i=1}^{bs} \min \left(\frac{(\det \nabla \Phi[\vec{x}_i] - 1)^2}{\det \nabla \Phi[\vec{x}_i]}, \tau \right),$$

$$L_{\mathcal{F} \rightarrow \mathcal{B}}^{\text{cycle}} = \frac{2}{bs} \sum_{i=1}^{bs/2} [\Phi_{\mathcal{B}}(\Phi_{\mathcal{F}}(\vec{x}_i)) - \vec{x}_i]^2$$



Cycle-Consistent INRs

Method: Complete Backward and Forward Terms

Data Loss:

$$L_{\mathcal{F}}^{\text{data}} = \frac{2}{bs} \sum_{i=1}^{bs/2} -\text{NCC}(S[\vec{x}_i], T[\Phi_{\mathcal{F}}(\vec{x}_i)]),$$

$$L_{\mathcal{B}}^{\text{data}} = \frac{2}{bs} \sum_{i=bs/2}^{bs} -\text{NCC}(T[\vec{x}_i], S[\Phi_{\mathcal{B}}(\vec{x}_i)]),$$

Cycle-consistent Terms:

$$L_{\mathcal{F} \rightarrow \mathcal{B}}^{\text{cycle}} = \frac{2}{bs} \sum_{i=1}^{bs/2} [\Phi_{\mathcal{B}}(\Phi_{\mathcal{F}}(\vec{x}_i)) - \vec{x}_i]^2$$

$$L_{\mathcal{B} \rightarrow \mathcal{F}}^{\text{cycle}} = \frac{2}{bs} \sum_{i=bs/2}^{bs} [\Phi_{\mathcal{F}}(\Phi_{\mathcal{B}}(\vec{x}_i)) - \vec{x}_i]^2,$$



Cycle-Consistent INRs

Method: Complete Regularization Tested

Jacobian determinant regularization:

$$L^{jac}[\Phi] = \frac{1}{bs} \sum_{i=1}^{bs} |1 - \det \nabla \Phi[\bar{x}_i]|.$$

Symmetric Jacobian determinant regularization:

$$L^{sjac}[\Phi] = \frac{1}{bs} \sum_{i=1}^{bs} \min \left(\frac{(\det \nabla \Phi[\bar{x}_i] - 1)^2}{\det \nabla \Phi[\bar{x}_i]}, \tau \right),$$

Bending Energy Penalty [5]:

$$\begin{aligned} L^{bend}[\Phi] &= \frac{1}{bs} \sum_{i=1}^{bs} \left(\left(\frac{\partial^2 \Phi[\bar{x}_i]}{\partial x^2} \right)^2 + \left(\frac{\partial^2 \Phi[\bar{x}_i]}{\partial y^2} \right)^2 + \left(\frac{\partial^2 \Phi[\bar{x}_i]}{\partial z^2} \right)^2 \right. \\ &\quad \left. + 2 \left[\left(\frac{\partial^2 \Phi[\bar{x}_i]}{\partial x \partial y} \right)^2 + \left(\frac{\partial^2 \Phi[\bar{x}_i]}{\partial x \partial z} \right)^2 + \left(\frac{\partial^2 \Phi[\bar{x}_i]}{\partial y \partial z} \right)^2 \right] \right), \end{aligned}$$



Cycle-Consistent INRs

Method: Inference – Taylor Expansion

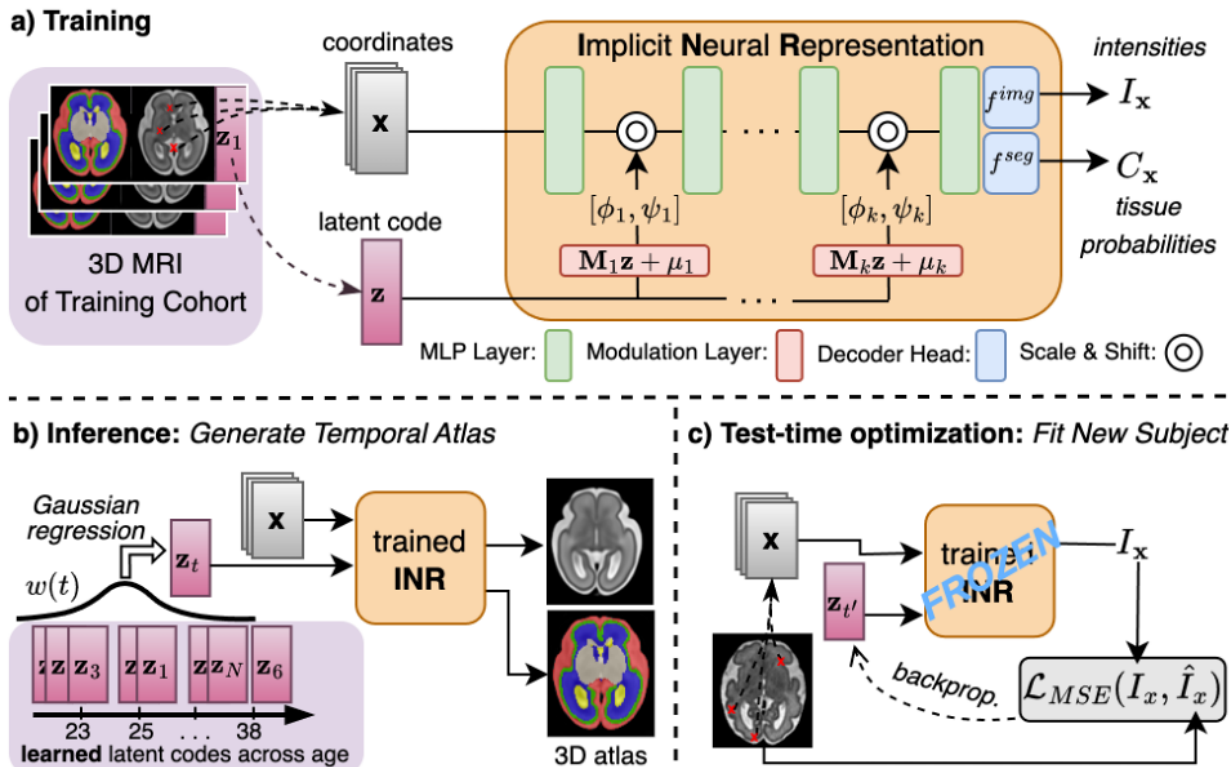
$$\begin{aligned}\Phi_{\mathcal{B}}^{-1}(\vec{x}) = & \Phi_{\mathcal{B}}^{-1}[\Phi_{\mathcal{B}}(\Phi_{\mathcal{F}}(\vec{x}))] + \\ & \nabla\Phi_{\mathcal{B}}^{-1}[\Phi_{\mathcal{B}}(\Phi_{\mathcal{F}}(\vec{x}))] \cdot (\vec{x} - \Phi_{\mathcal{B}}(\Phi_{\mathcal{F}}(\vec{x}))) + \\ & \frac{1}{2}\nabla^2\Phi_{\mathcal{B}}^{-1}[\Phi_{\mathcal{B}}(\Phi_{\mathcal{F}}(\vec{x}))] \cdot (\vec{x} - \Phi_{\mathcal{B}}(\Phi_{\mathcal{F}}(\vec{x})))^2.\end{aligned}$$

Can be simplified to:

$$\begin{aligned}\Phi_{\mathcal{B}}^{-1}(\vec{x}) = & \Phi_{\mathcal{F}}(\vec{x}) + \\ & \nabla^{-1}\Phi_{\mathcal{B}}(\Phi_{\mathcal{F}}(\vec{x})) \cdot (\vec{x} - \Phi_{\mathcal{B}}(\Phi_{\mathcal{F}}(\vec{x}))) + \\ & \frac{1}{2}\nabla^{-2}\Phi_{\mathcal{B}}(\Phi_{\mathcal{F}}(\vec{x})) \cdot (\vec{x} - \Phi_{\mathcal{B}}(\Phi_{\mathcal{F}}(\vec{x})))^2,\end{aligned}$$



CINA: Conditional Implicit Neural Atlas



Source [8]

